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## 电纺技术在生物医学中的应用进展

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**摘要:** 电纺技术已经成为结合多组分化合物与织造技术的关键工具, 可改变电纺丝材料的化学、物理和生物特性, 使其与不同的应用环境相适应。通过电纺技术制作的功能化纳米电纺丝材料, 在组织工程、创伤敷料、酶的固定化和药物(基因)载体等生物医学方面得到了广泛的应用。新型的电纺技术可以进一步优化纳米电纺丝的特性, 如同轴电纺、二相电纺技术; 电纺丝膜的修饰也为调控电纺丝的各向异性和多孔性提供了有效的方法。该文将概述功能化电纺丝的纺织技术及修饰方法在生物医学领域的研究与应用进展。

**关键词:** 电纺技术; 纳米纤维; 修饰; 生物医学应用

**中图分类号:** N39; TB383 **文献标识码:** A

## Electrospun technique for biomedical applications

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**Abstract:** Electrospun technique has become the pivotal tool, which is a combination of multi-component compositions and fabrication techniques. The chemical, physical and biological properties of electrospun scaffolds can be adjusted by the fabrication techniques to match the different environment that the scaffolds applied in. Functional nanofibrous scaffolds produced by electrospinning have great potential in many biomedical applications, such as tissue engineering, wound dressing, enzyme immobilization and drug (gene) delivery. The property of the nanofibrous scaffold can be further improved with innovative development in electrospinning processes, such as coaxial electrospinning and two-component electrospinning. Post modifications of electrospun membranes also provide effective means to render the electrospun scaffolds with controlled anisotropy and porosity. In this article, we will review the techniques and post modification methods of functional electrospun nanofibrous scaffolds applied in biomedical fields.

**Key words:** electrospinning techniques; nanofibrous; modification; biomedical applications

电纺丝技术的发展基于高压静电场下导电液体产生高速喷射的原理。在喷射熔体或溶液上通入几十千伏的交流或直流电高压, 在喷丝头和接地极间瞬时产生一个极不均匀的电场。喷丝头处的电场力用以克服溶液本身的表面张力和粘弹性力, 随着电场强度的增加, 喷丝头末端呈半球状的液滴被拉成圆锥状, 此即 Taylor 锥。电场强度超过一临界值后, 电场力将克服液滴的表面张力形成射流。经过溶剂的挥发或熔体冷却最终在接收极得到亚微

米, 甚至纳米数量级的纤维, 这一特性是其他非织造纤维纺织技术所不具备的<sup>[1]</sup>。纳米电纺丝具有高的比表面积、可调控的孔径和延展性, 从而能将其制成各种尺度和形状; 另外电纺丝的组成成分具有可控性, 使其具有不同的特性和功能, 因此该技术

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受到普遍的关注,如各种不同成分<sup>[2]</sup>的材料已被应用于过滤<sup>[3]</sup>、光学或化学传感器<sup>[4]</sup>、电极材料<sup>[5]</sup>和生物支架材料<sup>[6]</sup>。在生物医学应用领域,电纺丝已被用于组织工程材料<sup>[7]</sup>、酶和催化剂的固定化材料<sup>[8]</sup>、伤口敷剂<sup>[9]</sup>和人工血管<sup>[10]</sup>,以及用于防止术后诱导的伤口黏连<sup>[11]</sup>、可控药物或基因释放载体<sup>[12]</sup>等。本文概述近年来新的电纺技术与纺丝表/界面的修饰方法,及其它们在生物医学领域的应用进展。

### 1 电纺新技术在生物医学中的应用

纺织过程对电纺丝的性质和功能具有重要影响,利用不同的纺织方法,能够控制纤维的直径、形态和孔径。纳米纺丝材料必须具有特定的物理、生物特性,如在组织工程中,电纺丝除了必须具有适宜的机械性能以及能够模拟细胞外基质的纳米结构,还必须能够促进细胞贴附、扩散和增殖。对于创伤敷料,纳米纤维不但要作为组织再生的基底,而且在康复期间还要可控地释放某些生物活性成分或药物(如抗生素)。

**1.1 纤维定向排列的电纺技术** 在电纺丝制备中由于喷丝的速度非常快,收集到的纤维多呈无规则排布(非织造结构),但有时需要纤维定向排列以获得特殊的生物功能。定向收集电纺纤维的方法包括:辅助电场法<sup>[13]</sup>、薄轮收集法<sup>[14]</sup>、框架收集法<sup>[15]</sup>和机械拉伸法等4种。虽然机械拉伸法(单轴拉伸或双轴拉伸)是制作纤维定向排列常用的方法<sup>[16]</sup>,但随着拉伸程度的增加,纤维的孔隙率将随之下降。Yang等<sup>[17]</sup>报道了一种新的收集方法,在聚乙烯醇[poly(vinyl alcohol),PVA]电纺丝中加入少量的磁性颗粒,然后利用磁场即可获得定向排列的电纺丝纤维。Xu等<sup>[18]</sup>应用定向排列技术制备了聚丙交酯-己内酯[poly(l-lactide-co-ε-caprolactone),P(LLA-CL)]纳米纤维,研究了人冠状动脉平滑肌细胞在其上的

贴附、排列分布和迁移情况。Zong等<sup>[19]</sup>研究探讨了定向型聚丙交酯(poly-(L-lactide),PLLA)电纺丝的结构和其对心肌细胞生长的影响。Wang等<sup>[20]</sup>报道了制作具有纺织样结构和形态的聚己内酯(poly(ε-caprolactone),PCL)电纺丝膜的方法,其机械和生物特性均比随机排列的电纺丝要好,可作为潜在的组织工程材料。Wang等<sup>[21]</sup>制备了高度定向排列的PLLA电纺丝纤维表面(图1A),探讨了第九期鸡胚胎背根部神经中枢细胞和老鼠施旺细胞在材料表面的体外生物学活性,结果表明:神经突沿定向纤维和交叉纤维排列方向均生长,但神经突有时会被交叉纤维阻断(图1B);施旺细胞在高定向排列的电纺丝上生长呈双极性,高浓度纤维会导致神经突浓度升高,但神经突的平均长度在不同纤维浓度下是相同的(图1C)。

**1.2 多层电纺技术和混合电纺技术** Kidoaki等<sup>[22]</sup>用多层电纺和混合电纺两种新的电纺技术制备含有不同聚合物的合成纤维(图2),在多层电纺技术中,每种聚合物都被纺织成单层,不同聚合物层再被连续地收集到同一块平板上(图2a);在混合电纺技术中,两种不同的聚合物溶液同时从两个针头在不同的加工条件下喷出,在同一个收集器上形成混合纤维网(图2b)。多层电纺技术已制作出包含有聚亚胺酯层、明胶、I型胶原层的三层纳米电纺丝结构的纺丝材料。Tuzlakoglu等<sup>[23]</sup>制作的纳米和微米结合纤维已用于骨组织工程。Park等<sup>[24]</sup>将电纺技术与聚合物融合直接沉积技术(direct polymer melt deposition, DPMD)相结合,制作的纳米与微米混合的多层三维结构纤维,已用于组织再生。多层电纺丝已被用于引导骨组织再生<sup>[25]</sup>、止血<sup>[26]</sup>等方面的研究。

Baker等<sup>[27]</sup>用混合纺丝技术制作了一种聚己内

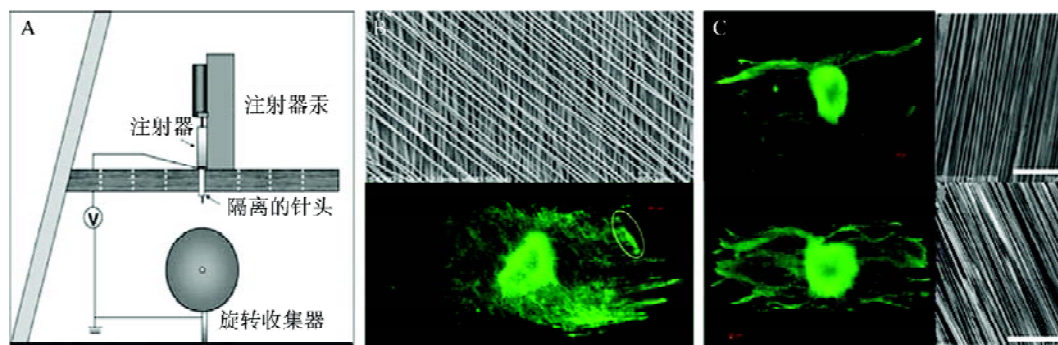


图1 A 高定向排列纤维制作装置; B 老鼠施旺细胞在交叉纤维上的生长情况;  
C 老鼠施旺细胞在不同浓度的纤维上生长情况

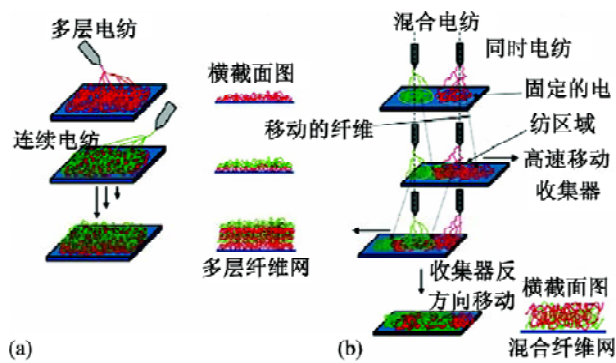


图2 (a)多层电纺和(b)混合电纺的原理图

酯/聚氧化乙烯(poly( $\epsilon$ -caprolactone)/poly(ethylene oxide), PCL/PEO)混合纤维,这种纤维是单向排列的,在水溶液中溶解掉PEO,得到了孔隙率增大的PCL定向排列的电纺丝材料。这种材料能增加间充质干细胞的渗透和分布,此外细胞的形态还具各向异性。

**1.3 双重孔结构材料的电纺技术** 通过加入黏土纳米颗粒可以增强聚合物基体的强度、硬度、抗热性和机械、物理性能。Lee等<sup>[28]</sup>利用电纺技术将包含聚乳酸[poly(lactic acid), PLA]、溶剂、黏土纳米颗粒和盐的悬浮混合液电纺出复合纳米纤维材料。再经盐过滤/鼓泡过程,形成一种独特的PLA/纳米黏土双重孔结构的合成纤维材料;具有三维结构的骨架材料,在缠绕的纤维缝隙中含有纳米级的孔,还含有由盐颗粒和气泡形成的微米级的大孔(50—300  $\mu\text{m}$ )。该结构适于组织再生,大孔能让特定的细胞通过(数百微米级),小孔结构能允许小分子物质(如营养物质、生长因子)渗透进入。但是双重孔结构材料的生物活性还没有被报道过。García-González等<sup>[29]</sup>用超临界抗溶剂技术将 $\text{TiO}_2$ 或羟基磷灰石(hydroxyapatite, HAP)分别填充于聚甲基丙烯酸酯/聚己内酯(poly(methylmethacrylate)/poly( $\epsilon$ -caprolactone), PMMA/PCL)或L-PCL电纺丝中,制成可用于组织工程的多孔材料。

**1.4 二相电纺技术** 该技术提供了一种在纤维中包裹小分子和(或)大分子的可行方法,被包裹的生物活性分子(药物或蛋白质)可以固定较长时间且可控释放。因此,该电纺技术在药物载体和组织工程领域比其他电纺技术具有更多的优势。Chew等<sup>[30]</sup>将牛血清白蛋白(bovine serum albumin, BSA)填充于人神经生长因子(nerve growth factor, NGF)里使其固定,再将两者包裹于聚己内酯-乙基乙烯磷酸盐

[poly( $\epsilon$ -caprolactone-co-ethyl ethylene phosphate), PCLEEP]电纺丝中(图3),使得神经生长因子持续释放三个月以上。Sanders等<sup>[31]</sup>将溶于二氯甲烷的聚乙烯-乙酸乙烯酯[Poly(ethylene-co-vinyl acetate), PEVA]和溶于磷酸缓冲液(PBS)的牛血清白蛋白(BSA)两种不相溶溶液,以40:1的比例混合制备出二相结构纤维,水相(PBS中的BSA)被包裹在PEVA中。

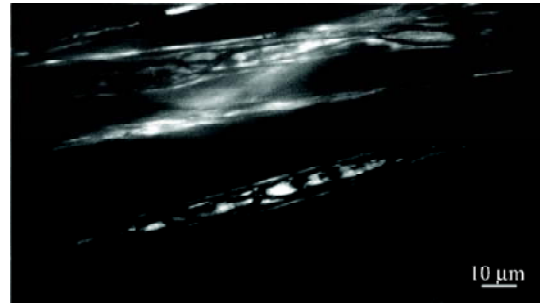


图3 包裹于PCLEEP电纺丝中蛋白质(NGF/BSA)的荧光图像

**1.5 同轴纤维的电纺技术** Sun等<sup>[32]</sup>首先报道了同轴纤维电纺技术,该技术的关键是将两个不同口径的针头套在一起组成同轴针头,两种聚合物不经直接混合就被一起电纺,适于制备表面修饰纳米纤维、功能性纳米材料,以及连续的中空纤维。它的优点是可以使一些难以加工的不同聚合物被纺织成具有外壳/内核结构的同轴纤维<sup>[33]</sup>;纤维外面的壳可以在电纺过程中保护核中的材料,当用生物活性物质来制作纳米纤维时这一特性更具有吸引力。Zhang等<sup>[34]</sup>以PCL为壳/明胶作为核制备出可生物降解的同轴电纺丝材料。Jiang等<sup>[35]</sup>用聚 $\epsilon$ -羧基乙酸内酯作为壳,以右旋糖苷与BSA作为核制备电纺纤维材料,在壳的保护和右旋糖苷的帮助下,BSA在电纺过程中几乎没有受到损伤,且核壳结构的形成还有助于BSA的可控释放。Zhang等<sup>[36]</sup>利用该技术在PCL电纺丝纤维表面包被上了胶原,有助于提高其与成纤维细胞的生物相容性;Zhang等<sup>[37]</sup>进一步在PCL电纺丝中包埋偶联异硫氰酸荧光素(fluorescein isothiocyanate, FITC)的牛血清白蛋白(BSA),达到了续释放的效果。Yang等<sup>[38]</sup>利用该技术对溶菌酶进行包被,酶并没有明显的变性,加工过程对酶二级结构的影响要比超声波所引起的要小。

除了能够保护蛋白质外,壳结构还能够保护活体细胞,因此同轴电纺又被称为细胞电纺技术。

Townsend-Nicholson和Jayasinghe<sup>[39]</sup>用聚二甲基硅氧烷(polydimethylsiloxane, PDMS)作为保护壳、细胞悬浮液为核,在两种不同流动速率下制得同轴纤维,结果表明由罗丹明6G染色的细胞经同轴电纺后被PDMS很好地包裹,且没受到任何损伤。Abeyewickreme等<sup>[40]</sup>用同轴电纺技术包裹老鼠胚胎干细胞,培养6d后用偶联了异硫氰荧光素酶(FITC)抗老鼠阶段特异性胚胎抗原1(stage specific embryonic antigen 1, SSEA-1)抗体染色的鼠胚胎干细胞,经过电纺的鼠胚胎干细胞与正常细胞都表达了SSEA-1,表明电纺包裹并没有影响老鼠胚胎干细胞的多潜能性。该技术提供了通过直接操作胚胎干细胞形成非特异组织的全新方法。此外,Salalha等<sup>[41]</sup>将细菌和病毒包埋于PVA电纺丝中并保持其活性;Yow等<sup>[42]</sup>在甲基化的胶原蛋白电纺丝里包埋了人间质细胞,并比接种于电纺丝表面的细胞具有更好的生物活性。

**1.6 助吹电纺技术** 至今大概有近百种聚合物被纺成电纺丝,然而,还有很多聚合物不能成功地应用于电纺<sup>[43]</sup>,如透明质酸(hexadecenoic acid, HA),由于其高黏度与高表面张力使其难以用于电纺,即使在低浓度下也不可行。助吹电纺技术的简单原理是,在针头旁边增加了空气流动。Um等<sup>[44]</sup>利用该技术成功地将透明质酸电纺成纳米纤维丝,助吹电纺技术具有四大优点:(1)空气流动产生的吹力和电场力可以克服聚合物溶液的高黏度与高表面张力;(2)对流动的空气加热可以进一步降低溶液的黏度,提高针头口的HA溶液喷丝的形成能力;(3)流动的空气可以加速溶剂蒸发,这是喷丝在到达收集器之前形成纤维一个很必要的条件;(4)通过控制空气温度和流速可以改变纤维直径,而纤维直径是纳米纤维膜物理特性的关键指标。基于这些优点,可利用助吹电纺方法加工一些至今还不能应用于电纺的聚合物;此外,该技术可显著地增加生产效率,适用于大规模制作。

## 2 电纺丝表/界面的修饰

虽然将不同的新电纺技术综合运用可以明显地提高纳米纤维的物理、生物特性,但是仍需要对电纺纳米纤维的表面进行修饰,使其在体内或临床应用中可以达到更好的效果,即通过在电纺丝表面修饰上合适的生物活性分子,可以使其具有更多必要的生物学特性,从而更好地应用于生物医学领域。电纺丝的修饰方法可大致分为化学修饰法和生物修

饰法。

**2.1 化学修饰法** Chua等<sup>[45]</sup>报道用肝细胞特异性半乳糖配体修饰PCLEEP纳米纤维表面后,可以用于肝细胞的培养。在肝细胞培养期间,肝细胞能通过半乳糖-唾液酸糖蛋白受体(asialoglycoprotein receptor, ASGPR)来贴附在纤维表面。结果表明:半乳糖修饰的纤维上生长的肝细胞比未修饰的纤维上生长的肝细胞具有更好的生物学特性。在半乳糖基化的电纺丝上生长的肝细胞嵌入了纤维中,而生长在半乳糖基化铸型膜上的肝细胞则呈球形。他们预测用半乳糖基化纳米纤维材料来固定肝细胞的方法对于设计人工肝脏辅助装置更为有利。

Roso等<sup>[46]</sup>将电纺和电喷射技术相结合,在聚乙烯电纺丝表面修饰上二氧化钛纳米颗粒。二氧化钛纳米颗粒可在电纺丝表面高度均匀分布,由于其具有光催化作用,电纺丝膜被证明是很好的催化剂。Luong等<sup>[47]</sup>在PLLA电纺丝表面修饰上羟基磷灰石改善了其亲水性。Prabhakaran等<sup>[48]</sup>用等离子体处理PCL电纺丝,改变了表面的生物相容性,有助于神经干细胞的生长。Jeong等<sup>[49]</sup>用氧气和等离子体处理蚕丝蛋白纤维,提高了其亲水性和细胞亲和性;Paneva等<sup>[50]</sup>在PCL电纺丝表面修饰了三氨基基团有助于降低电纺丝表面的硬度,同时降低电纺丝的熔融温度和结晶程度。Yao等<sup>[51]</sup>在聚氨酯(polyurethane, PU)电纺丝表面修饰上季铵盐基后发现具有抗菌作用。

**2.2 生物修饰法** Ma等<sup>[52]</sup>将明胶修饰到PET纳米电纺丝纤维表面,克服了PET表面的化学和生物学惰性,能够明显促进内皮细胞贴附、迁移和增殖而且能保持内皮细胞的形态。Wang等<sup>[53]</sup>证明醋酸纤维素电纺丝的表面经聚乙二醇修饰后能固定化酶,固定化酶的催化效能与活力均比自由酶高。Kim和Park<sup>[54]</sup>在聚丙交酯-乙交酯(poly(lactide-co-glycolide), PLGA)表面共价连接上了细胞贴附肽RGD(Arg-Gly-Asp),使细胞的贴附、迁移和分裂都得到了很大的改善。Yeo等<sup>[55]</sup>将胶原和蚕丝蛋白混合电纺,发现经过蒸汽处理后,交联的胶原蚕丝蛋白纤维更有助于正常人表皮角蛋白细胞(normal human epidermal keratinocytes, NHEK)和正常人表皮成纤维细胞(normal human epidermal fibroblasts, NHEF)的生长。Yang等<sup>[56]</sup>将聚碳酸酯电纺丝膜用于微流体免疫检测的基底,发明了一种新的检测HIV的方法,此方法可以提高HIV微流体免疫检测的灵敏度和信噪比。

基于同样的抗原抗体识别反应,微流体免疫检测还可以检测 AIDS 以外的疾病,如甲、乙、丙型肝炎,多种性病,许多严重的呼吸道疾病和禽流感。Tambralli 等<sup>[57]</sup>采用自组装技术将带有细胞连接肽(RGD)和基质金属蛋白酶 2(MMP-2)的两亲性短肽自组装入 PCL 电纺丝中,将两者的优点相结合提高了电纺丝生物活性。

我们实验室在材料修饰方面也做了一系列工作, Qin 等<sup>[58]</sup>应用疏水蛋白(HFBI)的特性,对亲水(云母)/疏水(PDMS)基底进行修饰,研究了修饰前后基底的亲/疏水变化,探讨了相应基底在免疫分析中的应用。Wang 等<sup>[59]</sup>利用原子力显微镜等研究探讨了 HFBI 蛋白修饰前后界面间的力,从而阐明 HFBI 修饰 PDMS 基底的机制。Hou 等<sup>[60]</sup>进一步应用微制作技术结合 HFBI 蛋白与胶原蛋白对 PDMS 表面进行图案化修饰,以上,结果表明:HFBI 改变了 PDMS 表面的疏水性,胶原有利于细胞的贴附生长,实现了细胞在 PDMS 表面图案化黏附与生长,且在转染试剂聚乙烯亚胺纤维素(polyethylenimine cellulose, PEI)存在下,带有绿色荧光蛋白(GFP)基因的质粒被转染入 293T 细胞并正常表达。

### 3 结论

综上所述,电纺技术相对于其他已有技术,它能够提供更多功能的、独特的纳米结构特性,纳米电纺丝材料在许多生物医学方面具有很好的应用前景。加工方法可进一步组合或改进产生新的纳米电纺丝;而适宜的生物活性物质对纳米电纺丝表面的修饰,是对纳米纤维进行功能调整使之更好地应用于生物医学领域的有效方法。

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